Abstract

The anterior cruciate ligament (ACL) is cited as the most frequently injured ligament in the knee. The standard treatment of ACL injury remains ligament reconstruction followed by a postoperative physiotherapeutic procedure. During the reconstruction, the torn ligament can be replaced with an autograft or an allograft. A synthetic ligament is also one of the available graft options. Synthetic grafts in ruptured ACL treatment have been used as scaffolds, stents, or prostheses. The story of using synthetic materials in ACL deficient knee treatment started in the beginning of the 20th century with the usage of silk and silver fibers. The second half of the 20th century abounded in new synthetic materials being proposed as torn ACL replacements, such as Supramid®, Teflon®, or Dacron®, Proplast®, carbon fiber graft, ABC graft, Kennedy-LAD®, Trevia, Leeds-Keio, Gore-Tex®, PDS®, EULIT®, and Polyflex® or LARS®. Artificial ligaments have intrigued surgeons for all these years as they represent the hope for grafts that are easily available and stronger than soft tissue “off-the-shelf” grafts, simplifying the surgery, and avoiding graft harvesting and donor site morbidity. However, most of the artificial grafts have been characterized by high rates of failure. One of the very few synthetic grafts gaining more widespread popularity has been LARS®. However, it is suggested that the ligament not be considered as a potential graft for primary reconstruction of the ACL, and it should be rather treated as an alternative graft in special cases, so the optimal synthetic graft material remains controversial.

Key words: artificial ligament, ligament prostheses, ligament reconstruction
The anterior cruciate ligament (ACL) is cited as the most frequently injured ligament in the human knee. In the USA, the average incidence frequency of ACL injuries amounts to 200,000 cases per year. The injuries most commonly occur in physically active individuals while playing multidirectional sports. For patients wishing to return to sports activities, the standard treatment for ACL injury is the reconstruction of the ligament, followed by a postoperative physiotherapeutic procedure. The aim of the reconstruction is reinstating functional knee stability, and in turn, reducing the risk of secondary injuries, such as further damage to the menisci and degenerative osteoarthritis. A recent analysis of epidemiological data shows an increase of the incidence of ACL ruptures and subsequent reconstructions.

**Anterior cruciate ligament (ACL) of the knee joint**

The ACL is one of the intra-articular ligaments of the knee joint. The ACL and the posterior cruciate ligament (PCL) are the most important stabilizers in the sagittal plane of the knee as they aim to stabilize the joint against the large anterior-posterior shear forces occurring while walking or running. “Cruciate”, literally meaning “cross”, and describes the shape of the ACL and PCL as they interconnect the tibia with the femur. The ACL attaches to a facet on the anterior part of the intercondylar area of the tibia and ascends posteriorly where it is attached to a facet at the back of the lateral wall of the intercondylar fossa of the femur. Functionally, the ACL consists of 2 distinct bundles that are characterized by a spatial relationship throughout the knee flexion: the anteromedial (AM) and posterolateral (PL) bundles. The bundles also play different roles in the biomechanics and stability of the joint. Some authors have distinguished a 3rd bundle in the anatomy of the ACL, the intermediate (IM) bundle. The ACL aims to resist anterior displacement and excessive rotation of the tibia relative to the femur.

**ACL injury and its treatment**

The ACL injury mechanism involves a combination of large rotational, side-to-side, and hyperextension forces through the knee. During the reconstruction, the torn ligament can be replaced with an autograft or an allograft. Synthetic ligament usage is also one of the available graft options. Autograft choices involve the patellar, hamstring, and quadriceps tendons, while the allograft options consist of the quadriceps, patellar, Achilles, hamstring, and anterior and posterior tibialis tendons, and the fascia lata. Shorter surgical and anesthesia time, fewer postoperative complications, reduced morbidity at the harvest site, faster postoperative recovery and lower incidence of postoperative arthrofibrosis, and less postoperative pain are considered to be the main advantages of allograft usage for ACL replacement. On the other hand, allograft usage may be associated with higher rates of re-rupture, limited availability, a delayed healing and ligamentization process in comparison to autografts, risk of disease transmission and expenses. The synthetic materials being used in ACL reconstruction were introduced with an aim to improve the strength and stability of the graft immediately after the reconstruction, reduce donor site morbidity and eliminate the potential for disease transmission. However, the first artificial grafts were characterized by high rates of failure and synovitis reactivation, thus with advancing technology, new synthetic materials have been developed for ACL reconstruction.

**Artificial ligament usage in ACL reconstruction**

Synthetic grafts in ruptured ACL treatment have been used as scaffolds, stents, or prostheses. A scaffold, such as the carbon fiber scaffold ligament, was introduced with the purpose of stimulating fibrous tissue ingrowth, and contributes to the ultimate strength of the new ligament. An example of a synthetic stent is the Kennedy ligament augmentation device (LAD). An example of a prosthetic graft was the Gore-Tex graft, Stryker Dacron graft, or ABC graft.

**The first half of the 20th century**

The history of the use of synthetic materials to replace the ACL goes back to the year 1903, when prosthetic ligaments made of silk sutures were introduced by Fritz Lange of Munich. Four years later, Lange reported on 4 cases of patients with ACL deficiency whose knees were stabilized with the use of artificial ligaments made of silk in conjunction with the semitendinosus and semimembranosus muscle tendons placed extra-articularly. However, in 1918, Smith of Cardiff criticized the silk fibers, considering them to be the cause of synovitis in his patient, sharing the same opinion with Max Herz (1906), and confirming the failure of silk usage in isolation within the intra-articular environment. The answer to that was introducing a foreign body scaffold aiming to provide initial strength during ligament healing and re-growth, and utilizing in ACL reconstruction silk augmented with fascia by Max Fritz of Munich, followed by Karl Ludloff of Frankfurt in 1927. Another example of a synthetic material being used for ACL replacement was a loop of silver wire introduced by Edred Corner of London in 1914.
The second half of the 20th century

In 1949, Ruther of Germany introduced a synthetic ligament for ACL replacement made of a polyamide derivative, and named Supramid. Nevertheless, the results of treatment with the use of Supramid were disappointing.

After a successful implantation of Teflon grafts into dog knees, Olav Rostrup of Edmonton in 1959 started using the synthetic material in humans. He didn’t recommend Teflon or Dacron for wide-scale use as he considered synthetic materials to be rather supporting devices, instead of ligament replacements. Even so, the ligament replacement device named Dacron was made commercially available in the 1980s by Stryker, but production was finally discontinued in 1994 as the results of treatment with its use were not satisfying. An evaluation carried out by Wilk and Richmond (1993) of patients after ACL reconstruction with the use of Dacron revealed significant deterioration of the ligament failure rate from 20% 2 years postoperatively to 37.5% at 5 years. The high rate of graft failure was confirmed by Maletius and Gillquist (1997) in a 9-year follow-up, amounting 44%.

Another synthetic graft being used in the second half of the 20th century was a porous Teflon graft, named Proplast. Interestingly, it was one of the first synthetic graft materials approved by the Food and Drug Administration (FDA), however, the results of its clinical usage were not satisfying. Also, flexible carbon fiber was introduced as a synthetic graft material for ACL reconstruction. David Jenkins of Cardiff started to use them in the mid-1980s as a scaffold aiming to encourage the ingrowth of fibroelastic tissue and production of new collagen. Nevertheless, the occurrence of the fragmentation of carbon creating unsightly staining of the synovium and foreign body reaction was noted. In 1985, Angus Strover of South Africa didn’t notice any occurrence of carbon debris in the knee joint cavity when the carbon fibers were used with the remnants of the original ligament or within a fascia sheath.

When it comes to Poland, the wide-ranging studies concerning carbon fiber usage generally in knee surgery and knee ligament reconstructions, especially in ACL reconstruction, have been carried out mainly by Andrzej Górecki and Wojciech Kuś in the Clinics of Orthopedics and Traumatology of the Medical University in Warszawa in cooperation with the AGH University of Science and Technology in Kraków.

The mid-1980s also brought the ligament replacement named Activated Biological Composite (ABC). The ABC graft, being a combination of polyester and carbon fiber, was placed through anatomical bony tunnels. In the beginning, the ligament gained popularity, however, eventually became obsolete like other synthetic grafts.

An example of an ACL augmentation device was the Kennedy-LAD, made of polypropylene and introduced by Jack Kennedy of London in the late 1970s. The synthetic stent was sutured to an autologous graft and fixed to the bone at both ends, with the aim to support and protect the autologous graft during the healing phase, when the autologous tissue was the weakest. The LAD was a braid-like braid of propylene that was designed to protect the autogenous graft from excessive stresses, however it happened to stress the autologous graft, leading to failure. One polyester graft resembling LAD in design, but being placed in a nonanatomic position was Trevia. The Leeds-Keio was a polyester mesh graft designed in order to augment the autogenous graft that was placed through bony tunnels and fixed outside the tunnel with staples. A Murray et al. study reporting the long-term results of patients 10–16 years after ACL reconstruction with the use of the Leeds-Keio ligament revealed rather poor results with a high rate of ligament rupture and knee laxity. Also, LAD usage results indicted a high rate of postoperative complications and re-surgeries, as well as causing effusions and synovitis reactivation and autogenous graft delay. All in all, it was suggested not to use Leeds-Keio or LAD devices due to their poor outcomes.

Other examples of synthetic grafts were Gore-Tex, PDS, EULIT, and Polysilk. The Gore-Tex graft was a prosthetic graft that, theoretically, aiming to avoid the bending forces at the entrance to the femoral tunnel, was placed in a nonanatomic position over the top of the femur.

Ligament advanced reinforcement system (LARS)

One of the synthetic material grafts introduced in the second half of the 20th century was a graft made of polyester named Ligostic, which evolved to a non-absorbable synthetic ligament device made of terephthalic polyethylene polyester fibers, the Ligament Advanced Reinforcement System (LARS). The LARS is intensively cleaned with the aim to remove potential machining residues and oils to further encourage soft tissue in-growth and reduce the risk of reactive synovitis. The LARS consists of 2 parts, an intraarticular part and an extraarticular one. The ligament intra-articular portion/scaffold is built of multiple parallel fibers that are twisted at 90-degree angles. The part is composed of 2 longitudinal external rotation fibers without transverse fibers, being designed as an imitation of ACL anatomic structure. The extraarticular part is waved by longitudinal and transverse fibers with the aim to avoid ligament deformation. The short-term postoperative results of patients after ACL reconstruction with the use of LARS are very satisfying. A mean 2.5-year follow up carried out by Dericks in 1995 revealed encouraging results of treatment with the use of LARS. Also, a follow-up at a mean of 8 years reported by Parchi et al. in 2013 showed satisfying results reflected in no postoperative complication occurrence and only one case of LARS rupture. On the other hand, the follow-up of 10 years postoperatively carried out by Tiefenboeck et al.
revealed lack of subjective satisfaction in half of patients treated with the use of LARS, thus the authors suggested not to consider the ligament system as a potential graft for primary reconstruction of the ACL and rather treat it as an alternative graft in special cases.50

Summary

The story of using synthetic materials in ACL deficient knee treatment started in the beginning of 20th century with the usage of silk and silver fibers. The story of using synthetic materials in ACL deficient knee treatment started in the beginning of the 20th century with the usage of silk and silver fibers. The second half of the 20th century abounded in new synthetic materials being proposed as torn ACL replacements such as Supramid, Teflon or Dacron, Proplast, carbon fiber graft, ABC graft, Kennedy-LAD, Trevia, Leeds-Keio, Gore-Tex, PDS, EULIT, and Polyflex or LARS.

Artificial ligaments have intrigued surgeons for all these years as they represent the hope for grafts that are easily available and stronger than soft tissue “off-the-shelf” grafts, simplifying the surgery, and avoiding graft harvesting and donor site morbidity. However, most of the artificial grafts have been characterized by high rates of failures. One of the very few synthetic grafts gaining more widespread popularity and which remains in use as an augmentation device up to this day has been LARS. However, it is suggested that the ligament should not be considered as a potential graft for primary reconstruction of the ACL, but should be rather treated as an alternative graft in special cases, so the optimal synthetic graft material remains controversial.

References

26. Gördecki A. Przydatność włókien węglowych w śródstawowych rekon-
strukturach przedniego więzadła krzyżowego stawu kolanowego. 1983, Rozprawa doktorska, Akademia Medyczna w Warszawie.


